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Single-shell return-to-the-origin probability diffusion MRI measure under a non-stationary Rician distributed noise

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In a nutshell	Numerical integration	Non-stationary log-Rician bias	
Problem:	In order to numerically evaluate the RTOP integral, one	Let us presume that the random variable $\log S_i(\mathbf{x})$ fol-	
- The estimation of the Ensemble Average	can use a direct approach assuming that the element of the surface. ΔS is inversely proportional to the number	lows a non-stationary log-Rician distribution with the underlying parameters $A_i(\mathbf{x})$ and $\sigma_i(\mathbf{x})$.	

Propagator (EAP) and its related features such as the Return-To-the-Origin Probability (RTOP) measure requires a huge amount of densely sampled multiple-shell **q**-space data.

Solution:

- We analytically derive an alternative approach to retrieve the RTOP directly from a single-shell
 q-space data.
- We provide a closed-form solution to correct noise-induced bias using a non-stationary log-Rician statistics.

Single-shell ${\bf q}\mbox{-space}$ data



of gradients (i.e. $\Delta S \propto 1/N_g$)

$$\operatorname{RTOP}^{(1)}(\mathbf{x}) = C_{\tau} \frac{1}{N_g} \sum_{i=1}^{N_g} \left(-\frac{1}{b} \log E(\mathbf{q}_i) \right)^{-3/2}$$
$$= C_{\tau} b^{3/2} \left\langle \left(-\log E(\mathbf{q}_i) \right)^{-3/2} \right\rangle,$$

• $C_{\tau} = 8^{-1} (\pi \tau)^{-3/2}$ is a time-related constant.

Considering the second-order Taylor expansion of the expectation operator $\mathbb{E}\{f(X)\}$ given $f(X) = X^{-3/2}$ we obtain the approximation

$$\mathbb{E}\left\{X^{-3/2}\right\} \approx \frac{1}{\mathbb{E}\left\{X\right\}^{3/2}} \left(\frac{15\mathbb{E}\left\{X^2\right\}}{8\mathbb{E}\left\{X\right\}^2} - \frac{7}{8}\right),$$

and finally redefine direct $\operatorname{RTOP}^{(1)}$ formulation using a sample mean estimator $\mathbb{E} \{X^p\} = \langle (-\log E(\mathbf{q}_i))^p \rangle$

New solution

$$\operatorname{RTOP}^{(2)}(\mathbf{x}) = \frac{15}{8} C_{\tau} b^{3/2} \frac{\left\langle \left(\log E(\mathbf{q}_i)\right)^2 \right\rangle}{\left\langle -\log E(\mathbf{q}_i) \right\rangle^{7/2}}$$

underlying parameters $A_i(\mathbf{x})$ and $O_i(\mathbf{x})$.

Assuming the random variables $\log S_i(\mathbf{x})$ and $\log S_0(\mathbf{x})$ are independent we state that

$$\mathbb{E}\left\{\left(\log\frac{S_i(\mathbf{x})}{S_0(\mathbf{x})}\right)^2\right\} = \mathbb{E}\left\{\left(\log S_i(\mathbf{x})\right)^2\right\}$$

+ $\mathbb{E}\left\{(\log S_0(\mathbf{x}))^2\right\} - 2 \mathbb{E}\left\{\log S_i(\mathbf{x})\right\} \mathbb{E}\left\{\log S_0(\mathbf{x})\right\}.$

Given the asymptotic expansion of the expectation $\mathbb{E} \{ (\log S_i(\mathbf{x}))^2 \}$ we revise the the RTOP⁽²⁾ formulation to handle the non-stationary log-Rician statistics



a single-shell \mathbf{q} -space data

Figure 1: The RTOP estimation procedure.

Ensemble Average Propagator

Under the narrow pulse assumption, the EAP in real space, $P(\mathbf{R})$, is related to the diffusion signal attenuation $E(\mathbf{q})$ in the **q**-space domain by means of the Fourier transform

$$P(\mathbf{R}) = \int_{\mathbb{R}^3} E(\mathbf{q}) \exp(-2\pi j \mathbf{q}^T \mathbf{R}) d\mathbf{q},$$

- S(q) is the diffusion signal acquired at position q,
 S₀ is the baseline measured without a diffusion sensitization,
- **q** is the wave vector related to $b = 4\pi^2 \tau \|\mathbf{q}\|^2$ with τ being the effective diffusion time.

Return-To-the-Origin Probability



Experimental results



Figure 2: (a) The RTOP measure obtained using the p% samples (left) and the absolute error of the measures with reference to the fully-sampled data. (1) The genu of the corpus callosum (CC), (2) the anterior thalamic radiation and (3) the splenium of the CC.

The probability in the origin indicates the EAP feature that the molecules minimally diffuse within the diffusion time and it is referred to as the RTOP measure

RTOP = $\int_{\mathbb{R}^3} E(\mathbf{q}) d\mathbf{q}.$

Considering a more general model beyond the diffusion tensor, i.e. $E(\mathbf{q}) = \exp(-bD(\mathbf{q}))$, and assuming that the diffusion does not depend on the radial coordinate we can define the RTOP integral in a spherical system

RTOP =
$$\frac{\sqrt{\pi}}{4(4\pi^2\tau)^{3/2}} \int_0^{2\pi} \int_0^{\pi} (D(\theta,\phi))^{-3/2} \sin\theta \, d\theta \, d\phi,$$

- $D(\theta, \phi)$ is the apparent diffusion coefficient.

(b) Absolute components of the bias $\mathcal{B}(\mathbf{x})$ for $N_g = 27$. (c) The mean relative error and the standard deviation of the RTOP measure.

HCP MGH 1016 ($b = 1000, 3000, 5000, 10000 \text{ s/mm}^2$)



Figure 3: The RTOP measure for maximal *b*-values.

Table 1: The correlation coefficient between the RTOP measures estimated under different maximal *b*-values (top) and under different techniques for same maximal *b*-value (bottom).

	3k/5k s/mm ²	$3k/10k \text{ s/mm}^2$	$5k/10k \text{ s/mm}^2$
MAP-MRI	0.900	0.859	0.942
MAPL	0.876	0.760	0.853
Direct	0.597	0.548	0.639
Refined	0.929	0.850	0.945

	$3k \text{ s/mm}^2$	$5k \text{ s/mm}^2$	$10k \text{ s/mm}^2$
Refined/MAP-MRI	0.902	0.926	0.889
Refined/MAPL	0.897	0.904	0.941
MAP-MRI/MAPL	0.776	0.842	0.809